Sampling and Visualizing Creases with Scale-Space Particles [Kindlmann-VIS-2009]

Please interrupt me with questions!



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Outline

Introduction: motivation, example, contributions

Method: interpolation, features, energy, visualization, computation

Results: lung CT, brain DTI, more

Discussion: scale, particles, analysis, future





Context & Motivation

Medical imaging is for measuring

Need to extract image features





Feature geometry is a computational proxy for anatomy

Lung CT: find airways, measure radii, study emphysema

Brain DTI: find major WM tracts, measure Fractional Anisotropy (FA), study psychiatric disorders

DTI not just for tractography

Much of it for FA studies



Want to create general way to detect and sample image features



3D Images





hatomy ohysema ional Anisotropy

[Smith-TBS-2006]

Ridges & Valleys = Creases [Eberly-JMIV-1994] [Eberly-1996] **Constrained** extremum $\{\mathbf{e}_i\}$ 2 Gradient g Hessian eigensystem e_i, λ_i λ_{z} Crease: g ortho to one or more e_i Eigenvalue gives strength Ridge surface: $\mathbf{g} \cdot \mathbf{e}_3 = 0$; $\lambda_3 < \text{thresh}$ e.g.: Ridge line: $\mathbf{g} \cdot \mathbf{e}_3 = \mathbf{g} \cdot \mathbf{e}_2 = 0;$ $\lambda_3, \lambda_2 < \text{thresh}$ Valley surface: $\mathbf{g} \cdot \mathbf{e}_1 = 0$; λ_1 > thresh

Feature sampling examples Using Visible Human, Female CT hand The different features: Isosurface Laplacian zero-crossing Ridges & Valleys ("creases") surfaces or lines **Same** code, different optimization each little glyph = one particle show local feature ingredients Sample features a **single scale**



Isosurface



AKA isocline, isophote, isocontour, level set $f(\mathbf{x}) = v_0$

Different, Cropped 3D view with 2D cutting plane

Laplacian 0-crossing



Classical definition of edge $\nabla^2 f(\mathbf{x}) = 0$; strength = $|\nabla f(\mathbf{x})|$

Ridge Surface



Ridge Line



Maximal curve wrt Hessian minor, medium eigenvecs $\nabla f(\mathbf{x}) \cdot \mathbf{e}_3(\mathbf{x}) = 0, \nabla f(\mathbf{x}) \cdot \mathbf{e}_2(\mathbf{x}) = 0; \text{ strength} = -\lambda_2$

Valley Surface



Minimal surface wrt Hessian major eigenvector **e**₁ $\nabla f(\mathbf{x}) \cdot \mathbf{e}_1(\mathbf{x}) = 0$; strength = λ_1



Valley Line



Minimal curve wrt Hessian major, medium eigenvectors $\nabla f(\mathbf{x}) \cdot \mathbf{e}_1(\mathbf{x}) = 0, \nabla f(\mathbf{x}) \cdot \mathbf{e}_2(\mathbf{x}) = 0; \text{ strength } = \lambda_2$





Particles for DTI **visualization** (earlier "Glyph Packing" [Kindlmann-VIS-2006]) Glyphs for diffusion tensors Sampling whole field Image for humans to look at Particles for DTI **analysis** (more recent [Kindlmann-VIS-2009]) Glyphs for Hessians of FA Sampling crease features Geometry for measurement

Why scale-space ...



Why scale-space ...

goal: sample middle of torus



Why scale-space ...

Particles sampling ridge lines

Glyphs displaying Hessians

Sca across sampling ridges particles



Particle-Image energy as function of feature strength

Hermite spline

























The purpose is not pretty pictures, it is feature sampling (visually debugged)

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Feature localization and sampling in space and scale

Glyphs displaying scale

Contributions

Efficient interpolation of scale for 3D images

Particle-based sampling of ridges and valleys, in scale-space (vs. implicit surfaces, at single scale) Energies that implement scale-localization

Glyphs for depicting Hessians and/or scale

Scale-space feature extraction in DTI

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Method Overview

Governing equation

Interpolation: discrete to continuous, scale & space

Crease feature constraints and strengths

Particle-Image energy

Inter-particle energy

System visualization and dynamics

, scale & space gths

Governing equation



scale

Feature constraints: enforced without contributing to energy

Population control (finding N) becomes side-effect of energy minimization

Inter-particle energy: induces uniform **spatial** sampling

Scale-Space

From '90s computer vision Image and all possible **blurrings** More general than multi-resolution methods: scale is **continuous**





Structures of different sizes are naturally extracted at different scales [Lindeberg-IJCV-1998]

Scale-Space And Diffusion

Various considerations lead to blurring with a Gaussian Image L(x) diffuses for time $t \rightarrow \text{continuum of images L}(x;t)$

$$L(x;t) = (L(\cdot) \star g(\cdot;t))(x) = \int g(\xi;t) d\xi$$
$$g(\xi;t) = \exp(-\xi^2/2t)/\sqrt{2\pi t}$$

Heat equation: 1st deriv. in time \rightarrow 2nd deriv. in space

$$\frac{\partial L(x;t)}{\partial t} \propto \frac{\partial^2 L(x;t)}{\partial x^2}$$

What's the analog in the **discrete** (implementation) domain?

$L(x-\xi)d\xi$

Lindeberg's Discrete Gaussian "Scale-Space for Discrete Signals" [Lindeberg-PAMI-1990] Beautiful analog to continuous Gaussian $L[i;t] = (f \star K[\cdot;t])[i] = \sum K[n;t]f[i-n]$ n $K[n;t] = \exp(-t)I_n(t); s = \sqrt{t} = "\sigma"$ $I_n(t)$ = modified Bessel function of order *n* $\frac{\partial K[i;t]}{\partial t} = \frac{1}{2} (K[\cdot;t] \star \begin{bmatrix} 1 & -2 & 1 \end{bmatrix})[i]$ $\Rightarrow \frac{\partial L[i;t]}{\partial t} = \frac{1}{2} (L[\cdot;t] \star \begin{bmatrix} 1 & -2 & 1 \end{bmatrix})[i]$ $\Rightarrow \frac{\partial L[i;s^2]}{\partial s} = s \left(L[\cdot;s^2] \star \begin{bmatrix} 1 & -2 & 1 \end{bmatrix} \right) [i]$



Lindeberg's Discrete Gaussian



Not the same as sampling a Gaussian Change **between** blurring levels important

Interpolate along scale

Want continuous scale, but hard with full-resolution volume images: have a memory limit

Sampling and reconstruction problem: how to pre-compute some blurrings and then accurately/efficiently interpolate?

Leverage Lindeberg's Gaussian:

Pre-compute blurrings of image L for discrete set of blurring levels

For intermediate scales, could linearly blend between, or

Knowing dL/ds at each scale, create cubic **Hermite spline**



- $\frac{\partial L}{\partial s} = s \left(L[\cdot; s^2] \star \begin{bmatrix} 1 & -2 & 1 \end{bmatrix} \right)$

Scale interpolation accuracy

- Goal: best accuracy with minimum number of preblurring volumes
- Measure error as squared difference between interpolated K[] and true K[], summed over support
- Optimize non-uniform scale sample locations by gradient descent on error



Hermite-spline scale interpolation makes scale-space practical for real-world 3D volumes



Uniform, Linear Uniform, Hermite Non-uniform, Linear Non-uniform, Hermite



Why not do it correctly?

I.e: reconstruct spatial image neighborhood around particle, at intermediate scale s (between pre-computed blurrings s₀, s₁)



Exact solution needs $(30 + N)^3$ samples Hermite-spline approximation needs 2(2 + N)³ samples Memory is slowest part of a computer

Spatial Interpolation

At each particle location:

Scale interpolation \rightarrow discrete spatial support

Separable convolution \rightarrow values and derivatives

6-sample support Piece-wise 6th-order polynomial C⁴ continuity Reconstructs cubics ("c4hexic" in Diderot) [Möller-TVCG-1997]



Particle-Image Energy E _i				
Ridge (R) and valley (V) surfaces (S) and				
		R L	R S	V L
	Definition	$\begin{array}{l}\mathbf{g}\cdot\mathbf{v}_2=0\\\mathbf{g}\cdot\mathbf{v}_3=0\end{array}$	$\mathbf{g} \cdot \mathbf{v}_3 = 0$	$\begin{array}{c} \mathbf{g} \cdot \mathbf{v}_1 = 0 \\ \mathbf{g} \cdot \mathbf{v}_2 = 0 \end{array}$
	λ sign	$\lambda_3 \leq \lambda_2 < 0$	$\lambda_3 < 0$	$0 < \lambda_2 \leq \lambda_1$
	Strength h	$- ilde{\lambda_2}$	$- ilde{\lambda_3}$	$\tilde{\lambda_2}$
	Tangent T	$\mathbf{v}_1 \otimes \mathbf{v}_1$	$\mathbf{v}_1 \otimes \mathbf{v}_1 + \mathbf{v}_2 \otimes \mathbf{v}_2$	$\mathbf{v}_3 \otimes \mathbf{v}_3$

$$E_i = e(f, \mathbf{x}_i, s_i) = -\gamma h(\mathbf{x}_i, s_i)$$

Particles migrate to **scale of** maximal feature strength as part of energy minimization (not a constriant)



Inter-particle Energy E_{ii}

$$E_{ij} = \Phi(r_{ij}, s_{ij}) = \Phi\left(\frac{|\mathbf{x}_i - \mathbf{x}_j|}{\sigma_r}, \frac{s_{ij}}{\sigma_r}\right)$$

No intrinsic orientation to particles' potential Have user-set "radii" in space σ_r and scale σ_s





 $= (1-\beta)\phi_c(r)b(s) + \beta b(r)b(s)s^2$

Inter-particle Energy E_{ij}



System Visualization

Glyphs at particle locations, possibly colormapped Glyphs show tensors related to local Hessian crease surfaces \rightarrow discs, lines \rightarrow rods Or, encode scale instead of Hessian eigenvalues





System Computation

Initialize with particle at every Nth voxel

"CPM: A Deformable Model for Shape Recovery and Segmentation Based on Charged Particles" [Jalba-PAMI-2004]

Sampling one vs. detecting all

Currently bottleneck

Every iteration decreases energy

Move particles, with spatial constraint

Periodically try adding or nixing particles

"Connected components" (CC)

Connected if non-zero inter-particle energy



(demo) (doesn't show scale-space)

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Lung CT Results

- Lung airway segmentation still not quite solved
- Particles captured 4-5 levels of branching, as well as size



Biggest



Lung CT Results



Smallest airways not much larger than voxels (benefit of working on continuous domain)

Brain DTI Results

Scale

Fractional Anisotropy (FA) ridge surfaces



Brain DTI Results



Without Scale-Space With Scale-Space

FA ridge lines



Double Point Load Stress Tensor Field



Teddy Bear







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Why not more Scale Space in Vis?

What are relative strengths, weaknesses of scale-space (with strength measures) versus topological simplification (with persistence measure)

Can always ask: but at what scale, and how stable with respect to scale?

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 \mathbf{S}

scale:





Joy of Particles

Map from crease definition to particle motion

Implement at level of individual particle behavior, watch group evolve

Same system for curves or surfaces, with or without scale space



Visualization or Analysis?

Intersection of both

Vis, by **methods** (particles, glyphs) and **modality** (CT, DT-MRI)

Vis & Analysis, by **strategy**: inspecting computation, feature detection, optimizing sampling

Analysis, by **goals**: quantitative studies of local properties, shape variation, registration



Applications since 2009



Helicity conservation by flow across scales in reconnecting vortex links and knots. MW Scheeler, D Kleckner, D Proment, GL Kindlmann, and WTM Irvine. *Proceedings of the* National Academy of Sciences, 111(43):15350–15355, October 2014.

Pulmonary lobe segmentation based on ridge surface sampling and shape model fitting. JC Ross, GL Kindlmann, Y Okajima, H Hatabu, AA Díaz, EK Silverman, GR Washko, J Dy, and R San José Estépar. Medical *Physics*, 40(12):121903, December 2013



(a) Selection of outliers





(b) Largest component



(d) Widget used for (b)

Open-Box Spectral Clustering: Applications to Medical Image Analysis. T Schultz and G Kindlmann. IEEE Transactions on Visualization and *Computer Graphics* (Proceedings of VIS 2013), 19(12):2100-2108, December 2013.

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Aarkers of Vascular Perturbation Correlate with Airway Structural Change in Asthma

Future work

Other kinds of features: Canny edges (should be possible with future Diderot!)

Varying sampling density (curvature, local size)

More parameter automation (did scale)

(maybe with Tuner?)

Meshing, where needed

GPU-based computation (also with future Diderot)

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Code online: http://people.cs.uchicago.edu/~glk/ssp/ (part of Teem) but unfortunately no GUI Maybe in Hale: https://github.com/kindlmann/hale Future grant may fund scale-space for Diderot Thanks for questions, feedback! GLK@uchicago.edu